Nuts & Bolts of Advanced Imaging

Image Reconstruction – Parallel Imaging

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No conflicts of interest to disclose

Outline

- § Noise correlation
- SNR scaled reconstruction
	- Obtaining images in SNR units
- Pseudo Replica Method
	- Determining the SNR (and g-map) for any parallel imaging reconstruction
- Iterative methods
	- Non-Cartesian Parallel Imaging
- Regularization in Iterative Methods

Noise in Parallel Imaging $r₂$ **Ira**

vuutX Idealized Experiment:

$$
\mathbf{s}=\mathbf{E}\boldsymbol{\rho}
$$

In practice, we are affected by noise

 $s = E\rho + \eta$

We can measure this noise covariance:

Psi = (1/(Nsamples-1))*(eta * eta'); Noise correlation % Matlab % eta:[Ncoils, Nsamples]

 \mathbf{v} Noise covariance matrix

C(*x^Nx*)

5

$$
\mathbf{s} = \mathbf{E}\boldsymbol{\rho} \qquad \qquad \Psi_{\Upsilon,\Upsilon'} = \langle \eta_{\Upsilon}, \eta_{\Upsilon'} \rangle
$$

Psi Examples – 32 Channel Coil

"Normal Coil" "Broken Coil"

Examination of the noise covariance matrix is an important QA tool. Reveals broken elements, faulty pre-amps, etc.

Noise Pre-Whitening \mathbf{v} *i*i iĝ

Solving Linear Equations: Solving Linear Faustions: $\sum_{n=1}^{\infty}$ Equations.

$$
\mathbf{A}\mathbf{x} + \boldsymbol{\eta} = \mathbf{b} = \begin{bmatrix} c_1 & c_2 \\ c_3 & c_4 \\ \hline c_5 & c_6 \end{bmatrix} \begin{bmatrix} x_1 \\ x_2 \end{bmatrix} + \begin{bmatrix} X_1 \\ X_2 \\ X_3 \end{bmatrix} = \begin{bmatrix} b_1 \\ b_2 \\ b_3 \end{bmatrix}
$$

$$
X_i : \text{Random value with zero mean } (\mu = 0) \text{ and variance } \sigma_i^2
$$

Suppose you know that:

$$
\sigma_3^2 = 5\sigma_1^2 = 5\sigma_2^2
$$

 $\frac{2}{2}$ Put less weight on this equation

We would like to apply an operation such that we have unit variance in all channels:

More generally, we want to weigh the equations with the "inverse square root" of the noise covariance, if

$$
\boldsymbol{\Psi} = \mathbf{L} \mathbf{L}^{\mathrm{H}}
$$

 = LL^H (20) We will solve: will solve:

$$
\mathbf{L}^{-1}\mathbf{A}\mathbf{x} = \mathbf{L}^{-1}\mathbf{b}
$$

Or:

$$
\mathbf{x} = \left(\mathbf{A}^{\mathrm{H}} \mathbf{\Psi}^{-1} \mathbf{A}\right)^{-1} \mathbf{A}^{\mathrm{H}} \mathbf{\Psi}^{-1} \mathbf{b}
$$

In practice, we simply generate "pre-whitened" input data before recon

Noise Pre-Whitening

Matlab:

```
%eta [Ncoils,Nsamples]
%psi [Ncoils,Ncoils]
%data [Ncoils,Nsamples]
%csm : Coil sensitivity map
psi = (1/(Nsamples-1))*(eta * eta');
L = chol(psi, 'lower');L inv = inv(L);
data = L inv * data;
csm = L inv * csm;%Now noise is "white"
%Reshape data and do recon
```
Noise covariance matrix

Example with test dataset

 $\overline{1}$ $\sqrt{2}$ 3 4 5 $\,6\,$ $\overline{7}$ $^{\rm 8}$ $\overline{5}$ $\overline{2}$ 3 $\overline{4}$ 6° $\mathbf{7}$ 8

At least two broken pre-amps

Noise Pre-Whitening – SENSE Example

White Noise "Normal Coil" "Broken Coil"

ismrm_demo_noise_decorrelation.m

SENSE – Image Synthesis with Unmixing **Coefficients**

SENSE – Simple Rate 4 Example

 $\tilde{\rho}(x_1) = \sum$ *Nc i*=0

 $u_i a_i$ $g(x_1) = \sqrt{\sum_{i=1}^{N_c} |u_i|^2} \sqrt{\sum_{i=1}^{N_c} |S_i|^2}$ *Nc i*=0 $|u_i|^2$ $\sqrt{\sum_{c}}$ *Nc i*=0 $|S_i|$ $\overline{2}$

SENSE g-factor

Reconstruction in SNR Units

Reconstruction Pipeline

Kellman et al., Magnetic Resonance in Medicine 54:1439 –1447 (2005)

Reconstruction in SNR Units $\overline{}$ $\overline{}$ b (21) and \mathbf{L}

Reconstruction Pipeline

Kellman et al., Magnetic Resonance in Medicine 54:1439 –1447 (2005)

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Reconstruction in SNR Units

Pseudo-Replica Method \overline{a} $\overline{$ 3 = 52
3 = 52
5 = 52 $\frac{1}{2}$ = $\frac{1}{2}$ 2 (19) – 19) – 19) – 19) – 19) – 19) – 19) – 19) – 19) – 19) – 19) – 19) – 19) – 19) – 19) – 19) – 19) – 19) –
2 (19) – 19) – 19) – 19) – 19) – 19) – 19) – 19) – 19) – 19) – 19) – 19) – 19) – 19) – 19) – 19) – 19) – 19) –

What if unmixing coefficients are never explicitly formed: explicitly formed: \mathcal{L} and \mathcal{L} (20) \mathcal{L} (20

ismrm_pseudo_replica.m

Pseudo-Replica Method – Example 256 trials

Advantage of Cartesian Undersampling

Cartesian Undersampling

"Random" Undersampling

To solve the general non-Cartesian case, we return to the original problem: $s = 1$

C(*x^Nx*)

$$
\mathbf{s} = \mathbf{E}\boldsymbol{\rho} \qquad \tilde{\boldsymbol{\rho}} = \arg\min_{\boldsymbol{\rho}} \left\{ \left\| \mathbf{E}\boldsymbol{\rho} - \mathbf{s} \right\|_2 \right\}
$$

It is not practical to solve with direct inversion in general.

But we can use a number of different iterative solvers to arrive at the solution

- the encoding matrix matrix \blacksquare . Each row in the encoding matrix represents encoding \blacksquare t_{eq} diants. • Conjugate Gradients
- **location in Figure 1. Parallel Imaging reconstruction in the task of Eq. 1. Parallel Imaging reconstruction is the task of Eq. 1. Parallel Imaging reconstruction is the task of** \mathbb{R} **and** \mathbb{R} **is the task of \mathbb{R}** location in *k*-space, i.e. equivalent to Eq. 1. Parallel Imaging reconstruction is the task of • LSQR (Matlab)

```
inverting the system of equations in Eq. ??, i.e.:
for x if A is consistent, otherwise it attempts t<br>squares solution X that minimizes norm(B-A*X)...
                       sistent, otherwise it attempts to solve the least \vertAFUN(X,'notransp') accepts a vector input X and returns the<br>matrix-vector product A*X while AFUN(X,'transp') returns A'*X. In all
                         inverting the system of equations in Eq. ?. ( ) is the system of equations in Eq. ?. ) is the system of equations in Eq. ?. ( ) is the system of equations in Eq. ?. ( ) i.e.: ( ) i.e
X = lsqr(A,B) attempts to solve the system of linear equations A*X=B<br>for X if A is consistent, otherwise it attempts to solve the least
X = lsqr(AFUN,B) accepts a function handle AFUN instead of the matrix A.
>> help lsqr
  lsqr lsqr Method.
     for X if A is consistent, otherwise it attempts to solve the least
     AFUN(X,'notransp') accepts a vector input X and returns the
```
E. All parallel include the parallel induction and solution and solution and solution to find some and solution to find of the following syntaxes, you can replace A by AFUN...

To use LSQR (or Conjugate Gradients), we "just" need to be able to write a function that does the multiplication with E and E ^H:

Let's first look at a simple Cartesian case

Multiplication with E^H

```
rho = zeros(size(csm)); %csm: coil sensitivities
%sampling mask: 1 where sampled, zero where not
rho(repmat(sampling mask, [1 1 size(csm, 3)]) == 1) = s(:);rho = ismrm transform kspace to image(rho,[1,2]);
rho = sum(conj(csm) .* rho, 3);
```
Multiplication with E

 $s =$ repmat(reshape(rho,size(csm,1),size(csm,2)),[1 1 size(csm,3)]) .* csm;

```
s = ismrm transform image to kspace(s, [1,2]);
```

```
s= s(repmat(sampling mask, [1 1 size(csm,3)]) == 1);
```
Iterative SENSE

If we have the multiplication with E and E^H implemented as a Matlab function:

```
function o = e cartesian SENSE(inp, csm, sp, transpose indicator)
% sp: sampling pattern
% csm: coil sensitivities
```
Iterative SENSE could be implemented as:

% s: vector of acquired data $E = \theta(x, tr)$ e cartesian SENSE(x,csm,(sp > 0),tr); $img = lsqrt(E, s, l = -5, 50);$ $img = reshape(imq, size(csm,1), size(csm,2));$

Cartesian SENSE Iterative SENSE

Quick note on the non-uniform FFT

To implement multiplication with E and E^H in the non-Cartesian case, we need to do the non-uniform Fourier transform $1,2$.

In this course, we will use Jeff Fesslers "nufft" package. We recommend you download the latest version from:

http://web.eecs.umich.edu/~fessler/irt/fessler.tgz

```
%k: k-space coordinates [Nsamples, 2], range –pi:pi
%w: Density compensation weights
%s: Data
%Prepare NUFFT
N = [256 256]; 8Matrix size
J = [5 5]; %Kernel size
K = N*2; 80versampled Matrix size
nufft st = nufft init(k,N,J,K,N/2,'minmax:kb');
recon = nufft adj(s \cdot * \text{repmat}(w,[1 \text{ size}(s,2)])), nufft st);
```
¹Keiner, J., Kunis, S., and Potts, D. Using NFFT 3 - a software library for various nonequispaced fast Fourier transforms. ACM Trans. Math. Software, 2009 2Fessler J and Sutton B. Nonuniform fast Fourier transforms using min-max interpolation. IEEE TSP 2003

To use LSQR (or Conjugate Gradients), we "just" need to be able to write a function that does the multiplication with E and E ^H:

Now we have the tools for the non-Cartesian case:

Multiplication with E^H

Iterative SENSE – non-Cartesian

If we have the multiplication with E and E^H implemented as a Matlab function:

```
function o = e non cartesian SENSE(inp, csm, nufft st, w, transpose indicator)
% nufft_st: From nufft_init
% csm: coil sensitivities, w: density compensation
```
Non-Cartesian SENSE could be implemented as:

Regularization - Basics

$$
\mathbf{A}\mathbf{x} = \mathbf{b} \qquad \qquad \mathbf{x} = \left(\mathbf{A}^{\mathrm{H}}\mathbf{A}\right)^{-1}\mathbf{A}^{\mathrm{H}}\mathbf{b}
$$

Adding constraints:

$$
\mathbf{x}_{\lambda} = \arg\min\left\{ \left\| \mathbf{A}\mathbf{x} - \mathbf{b} \right\|_{2} + \frac{\lambda \left\| \mathbf{L}(\mathbf{x} - \mathbf{x}_{0}) \right\|_{2}}{\lambda} \right\}
$$

L: Linear Transform X_0 : Prior Estimate

Solution:

$$
\mathbf{x}_{\lambda} = \mathbf{x}_0 + \left(\mathbf{A}^{\mathrm{H}}\mathbf{A} + \lambda^2 \mathbf{L}^{\mathrm{H}}\mathbf{L}\right)^{-1}\mathbf{A}^{\mathrm{H}}(\mathbf{b} - \mathbf{A}\mathbf{x}_0)
$$

An example

$$
\mathbf{x}_0 = 0 \qquad \qquad \mathbf{L} =
$$

$$
=\left[\begin{array}{c} \frac{1}{\sqrt{2}} & \frac{1}{\sqrt{2}} \\ \frac{1}{\sqrt{2}} & \frac{1}{\sqrt{2}} \\ \frac{1}{\sqrt{2}} & \frac{1}{\sqrt{2}} \end{array}\right]
$$

 \lfloor

1 $\rho_{\,2}^{}$

 $\ddot{}$

1 $\rho_{_N}$ $\overline{}$

 $\overline{}$

 $\overline{}$

 $\overline{}$

 $\begin{array}{c} \end{array}$

 $\overline{}$

SENSE, 12 coils

Regularization – Iterative Methods zation – Iterative Methods

<u>**x**</u> *x* (*ke ska2* (*sk2* (

⇢

$$
\tilde{\boldsymbol{\rho}} = \arg\min_{\boldsymbol{\rho}} \left\{ \left\| \mathbf{E} \boldsymbol{\rho} - \mathbf{s} \right\|_2 + \lambda \left\| \mathbf{L} \boldsymbol{\rho} \right\|_2 \right\}
$$

Equivalent to solving:

$$
\begin{array}{c}\n\text{Measured data} \longrightarrow \begin{bmatrix} \text{s} \\ \text{0} \end{bmatrix} = \begin{bmatrix} \text{E} \\ \text{L} \end{bmatrix} \rho\n\end{array}
$$

Regularized non-Cartesian SENSE could be implemented as: the encoding matrix \mathbf{r} row in the encoding matrix represents encoding matrix \mathbf{r}

```
% s: vector of acquired data
           of acquired data<br>
and the set of acquired data
% s: vector of acquired data<br>E = @(x,tr) e_reg_non_cartesian_SENSE(x, csm, nufft_st, w, tr);
img = lsqr(E, [s \cdot* repmat(sqrt(w),[size(csm,3),1]);zeros(imgele,1)], 1e-3,30);<br>img = reshape(img,size(csm,1),size(csm,2));
img = reshape(imq, size(csm,1), size(csm,2));
```
 $\overline{}$ ismrm_demo_regularization_iterative_sense.m

Regularization – Iterative Methods

ismrm demo regularization iterative sense.m

Regularization – Iterative Methods D_{α} zation – Iterative Methods

$$
\tilde{\boldsymbol{\rho}} = \arg\min_{\boldsymbol{\rho}} \left\{ \left\| \mathbf{E}\boldsymbol{\rho} - \mathbf{s} \right\|_2 + \lambda \left\| \mathbf{L}\boldsymbol{\rho} \right\|_2 \right\}
$$

SPIRiT Approach

k-space points can be synthesized from neighbors 2 $-$ 1 $-$

 $\mathbf{G}\mathbf{d} = \mathbf{d}$

= LL^H (23)

SPIRiT Approach \overline{C} (28) \overline{C} (2

We can formulate the reconstruction problem in *k*-space as:

$$
\tilde{\mathbf{x}} = \arg \min_{\mathbf{x}} \{ ||\mathbf{D}\mathbf{x} - \mathbf{y}||_2 + \lambda ||\mathbf{G}\mathbf{x} - \mathbf{x}||_2 \}
$$
\n
$$
\mathbf{x} : \text{Cartesian } k\text{-space solution.}
$$
\n
$$
\mathbf{D} : \text{Sampling operator (e.g. onto non-Cartesian } k\text{-space)}
$$
\n
$$
\mathbf{G} : \text{SPIRiT convolution operator}
$$
\n
$$
\text{Can be applied as multiplication in image space}
$$

Could also be sampling operator from image to *k-*space

Lustig and Pauly. Magn Reson Med. 2010

Spiral Imaging Example

ismrm_demo_non_cartesian.m

Summary

- Noise decorrelation is used to reduce the impact of varying noise levels in receive channels.
- SNR scaled reconstruction are a way to evaluate reconstructions directly on the images.
- Pseudo Replica Method allows the formation of SNR scaled images in methods where unmixing coefficients are not explicitly obtained
- Iterative methods can be used for both Cartesian and non-Cartesian methods
- Regularization can be added to iterative methods in a straightforward fashion

Acknowledgements

- Jeff Fessler
	- http://web.eecs.umich.edu/~fessler/code/
- Brian Hargreaves
	- http://mrsrl.stanford.edu/~brian/mritools.html
- Miki Lustig
	- http://www.eecs.berkeley.edu/~mlustig/Software.html

Download code, examples: http://gadgetron.sf.net/sunrise

EXERCISES

Load exercise data

load hansen exercises.mat whos

Reconstruct aliased images

Observations, noise?

Do SENSE reconstruction

- Calculate SENSE unmixing
- Apply unmixing

Generate noise covariance matrix

- noise color
- Observations, is this a good coil?

Do noise pre-whitening

help ismrm calculate noise decorrelation mtx help ismrm apply noise decorrelation mtx

Do SENSE reconstruction

- Compare to before prewhitening

Analyse FFT to image space.

- Scaling?
- How to set the scale factor

Do SENSE reconstruction

Create SNR image and g-map

Do 100 reps of SENSE recon (just unmixing part)

Calculate standard deviation of the noise

Create SNR image and g-map

Reconstruct aliased images using nufft

Setup encoding matrix anonymous function

ismrm encoding non cartesian SENSE.m

Reconstruct non-Cartesian SENSE

Explore non-Cartesian Demo

ismrm_demo_non_cartesian.m